Central Artery Stiffness in Hypertension and Aging
A Problem With Cause and Consequence

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Systemic hypertension is a risk factor for many diseases affecting the heart, brain, and kidneys. It has long been thought that hypertension leads to a thickening and stiffening of central arteries (ie, stiffness is a consequence), whereas more recent evidence suggests that stiffening precedes hypertension (ie, stiffness is a cause). We submit, however, that consideration of the wall biomechanics and hemodynamics reveals an insidious positive feedback loop that may render it irrelevant whether hypertension causes or is caused by central arterial stiffening. A progressive worsening can ensue in either case, thus any onset of stiffening merits early intervention.

Mechanical Foundations
Understanding arterial function requires integration of biological and mechanical information.1,4 Stress (a force intensity) is a key concept in biomechanics; it enables one to calculate the stiffness of a material and assess its strength. Mean circumferential stresses in arteries can be estimated using Laplace’s equation:

$$\sigma_\theta = Pa / h$$

where $P$ is pressure, $a$ is the pressurized luminal radius, and $h$ is the wall thickness. In vitro experiments reveal nonlinear pressure–radius relations, $P = \hat{P}(a)$, hence acute increases in blood pressure increase both wall stress (with $a$ increasing because of wall elasticity and $h$ decreasing because of the near incompressibility) and material stiffness (essentially the slope of the stress–stretch relationship). Such pressure-induced increases in material stiffness increase most clinical measures of the stress–stretch relationship. Such pressure-induced incompressibility and material stiffness (essentially the slope of the stress–radius relations, $P(\hat{R}(a))$, but problematic mechanobiologically (higher $\sigma_\theta$) and lower mean wall shear stress $\tau = \frac{4Q}{\pi a^3}$, where $\mu$ is viscosity and $Q$ volumetric flow rate). Increased circumferential stress promotes matrix synthesis, often via local production of angiotensin-II, and associated wall thickening; decreased wall shear stress downregulates endothelial nitric oxide, a vasodilator and anti-inflammatory mediator. Inflammation is an important contributor to arterial stiffening in hypertension and aging, which can be beneficial hemodynamically (lower PWV) but problematic mechanobiologically (higher $\sigma_\theta$ and lower mean wall shear stress $\tau = \frac{4Q}{\pi a^3}$). Increased circumferential stress promotes matrix synthesis, often via local production of angiotensin-II, and associated wall thickening; decreased wall shear stress downregulates endothelial nitric oxide, a vasodilator and anti-inflammatory mediator. Inflammation is an important contributor to arterial stiffening in hypertension and aging, which can be beneficial hemodynamically (lower PWV) but problematic mechanobiologically (higher $\sigma_\theta$ and lower mean wall shear stress $\tau = \frac{4Q}{\pi a^3}$).

Radius $a$ tends to increase in central arteries in hypertension and aging, which can be beneficial hemodynamically (lower PWV) but problematic mechanobiologically (higher $\sigma_\theta$ and lower mean wall shear stress $\tau = \frac{4Q}{\pi a^3}$). Increased circumferential stress promotes matrix synthesis, often via local production of angiotensin-II, and associated wall thickening; decreased wall shear stress downregulates endothelial nitric oxide, a vasodilator and anti-inflammatory mediator. Inflammation is an important contributor to arterial stiffening in hypertension and aging, which can be beneficial hemodynamically (lower PWV) but problematic mechanobiologically (higher $\sigma_\theta$ and lower mean wall shear stress $\tau = \frac{4Q}{\pi a^3}$).

The ratio $\tau_{\mu} Q(\pi a^3)$ also affects local (Equation 1) and global (Equation 2) biomechanics. It would need to increase to restore $\sigma_\theta$ toward normal in response to a chronic increase in pressure, which would be mechanobiologically favorable. Yet, such a change could increase PWV, which would be hemodynamically unfavorable because it could augment central pulse pressure. Hence, local and global mechanics could again be at odds unless a decrease in material stiffness ($E$ in Equation 2) offsets effects of an increased $\tau_{\mu} Q(\pi a^3)$. Most data suggest, however, that material stiffness remains nearly the same or increases in hypertension and aging.

Stiffening as a Consequence?
Because of the complexity and progressive nature of hypertension and its effects, animal models remain essential for collecting longitudinal information on biological and mechanical changes. Early work, in the 1950s to 1970s, suggested that sustained increases in blood pressure stimulate matrix synthesis and thus vascular thickness and structural stiffness.6,7 These findings seem to be supported by many subsequent animal studies even although often at the expense of increasing structural stiffness (essentially wall thickness times material stiffness).

Different metrics are used clinically to assess structural stiffness of central arteries, with carotid-to-femoral pulse wave velocity (cfPWV) the current gold standard.1,2 It is thought that an increased cfPWV causes the reflected pressure wave to return to the proximal aorta earlier in the cardiac cycle, which augments central pulse pressure. Albeit not strictly applicable, the Moens–Korteweg equation provides some intuition:

$$\text{PWV} = \sqrt{\frac{Eh}{2\rho a}}$$

where PWV denotes the speed at which the pressure wave propagates, $E$ is a material stiffness, $h$ and $a$ are thickness and inner radius, respectively, and $\rho$ is the density of the (assumed inviscid) blood that flows within a long vessel of uniform geometry and properties. With $Eh$ the structural stiffness, Equation 2 shows that increases in either material stiffness or wall thickness can impact the hemodynamics equally.
though most do not delineate cause and consequence because of imprecise comparisons of evolving pressure and wall properties. Nevertheless, in vivo aortic banding studies confirm that the aorta stiffens structurally in response to increased pressure, and by multiple animal studies. For example, structural stiffness is higher in aortas of young spontaneously hypertensive rats, because of, in part, a greater wall thickness, despite blood pressure being normal; pressure subsequently increases, however, despite differences in structural stiffness becoming less compared with controls. As noted earlier, this structural stiffening seems to occur without material stiffening, implying that intramural cells attempt to preserve material stiffness while offsetting increased pressure-induced stresses by thickening the wall. Although a definite proof of causality remains wanting, these animal- and population-based clinical studies suggest that stiffening can precede hypertension (stiffening is a consequence), typical via an increase in structural stiffness that adversely affects hemodynamics, despite possibly being initially favorable mechanobiologically.

Stiffening as a Cause?
Seminal work in the late 1990s suggested that “impaired elasticity [increased structural stiffness] of larger arteries is an antecedent factor in the natural history of BP [blood pressure] elevation at the population level.” This initial clinical finding has been supported by more recent population-based studies and by multiple animal studies. For example, structural stiffness is higher in aortas of young spontaneously hypertensive rats, because of, in part, a greater wall thickness, despite blood pressure being normal; pressure subsequently increases, however, despite differences in structural stiffness becoming less compared with controls. As noted earlier, this structural stiffening seems to occur without material stiffening, implying that intramural cells attempt to preserve material stiffness while offsetting increased pressure-induced stresses by thickening the wall. Although a definite proof of causality remains wanting, these animal- and population-based clinical studies suggest that stiffening can precede hypertension (stiffening is a consequence), again via an increased structural stiffness that adversely affects the hemodynamics while possibly being favorable mechanobiologically.

Cause and Consequence
The tendency in science and medicine is to seek simplicity. Hence, based on the preponderance of recent evidence we now find suggestions that, “vascular stiffness is a precursor rather than a result of hypertension” or “...support the hypothesis that arterial stiffness is a cause rather than a consequence of hypertension”. Nevertheless, the totality of clinical and experimental findings suggest that (1) induced hypertension can lead to stiffening and (2) de novo stiffening can lead to hypertension. The former is consistent with local mechanobiological responses to increases in pressure-induced wall stress; in humans, this may underlie many types of secondary hypertension. In contrast, the latter seems to initiate as a global hemodynamic response to diffuse antecedent structural stiffening; in humans, this may underlie many types of essential hypertension and aging. Notwithstanding the importance of understanding and controlling essential hypertension, whether central arterial stiffening is the cause or consequence of developing hypertension, progressive local mechanobiological responses and adverse global hemodynamic changes are expected in both cases. That is, a potentially insidious feedback loop could exacerbate both central artery stiffening and increasing blood pressure (Figure). The real problem, therefore, may be that changes in arterial properties are both cause and consequence, which is ultimately worse because of the possible positive feedback. We should thus be careful not to under estimate the clinical challenge.

Indeed, a similarly vicious feedback loop seems to link large and small arteries. In contrast to large arteries, small (resistance) vessels tend to increase the ratio $h/a$ in hypertension via an inward remodeling process (ie, decreased radius $a$), likely because of a mechanobiological myogenic response that is distinct to arterioles. This decrease in radius could help protect the microcirculation from increased pulse pressure-induced damage, yet it increases peripheral resistance to flow ($R=8\mu L/\pi a^4$, where $L$ is the length over which the pressure drops) and thereby increases mean arterial pressure. Again, local wall mechanics/mechanobiology and global hemodynamics/physiology can be at odds. Finally, roles of the initially stiffer medium-sized (muscular) arteries in hypertension and aging are less clear; these vessels tend not to change in caliber or stiffen further, which may also be favorable locally but detrimental globally. As central arteries stiffen, the normal gradient in stiffness from elastic-to-muscular arteries decreases and pressure waves propagate farther distally where they can damage the microcirculation of end organs despite inward remodeling of the resistance vessels.

Closure
Research over the past 15 years reveals that biomechanical properties of central arteries play fundamental roles in both the health of and the development and progression of disease in end organs. Hence, despite controversy over the best metric to use, central artery stiffness is an important diagnostic metric and a therapeutic target. Our interpretations based on physical–mathematical–biological concepts support these previous conclusions, but emphasize a greater concern. An insidious positive feedback loop between local mechanobiological responses and global hemodynamics may render central artery stiffening both a cause and a consequence of hypertension. Moreover, this situation can be exacerbated by a similarly
vicious cycle between large- and small-vessel remodeling, particularly when microvessels are damaged in the kidneys, which are fundamental to long-term blood pressure control.

The need for early intervention is thus acute, as is the need to identify strategies to prevent entry into these feedback loops before the elevation of blood pressure or pulse wave velocity. Clinically, arterial stiffness should be a mandatory measurement in any trial of lifestyle change or antihypertensive drug efficacy. Fundamentally, we must understand better the genetic basis of stiffness and early vascular aging, mechanisms of cellular sensing and regulation of the extracellular matrix that endows the wall with its biomechanical functionality and structural integrity, interactions between the mechanobiology and the inflammation, and inter-relations among large and small arteries, particularly those of the kidney. Toward this end, physical–mathematical–biological approaches promise to yield increased insight.

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References

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